The lateral edge of proton therapy beams: Clinical relevance and current developments

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Motivation

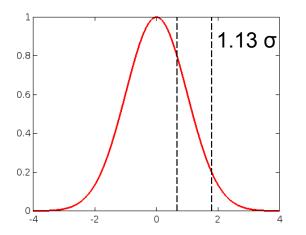
Having OARs immediately distal to the target may be risky due to:

- High weighting of distal spots (esp. in SFUD)
- Range uncertainty
- Increased LET / RBE at end of proton range

• Use of lateral edge to deliver dose to these areas may be preferable





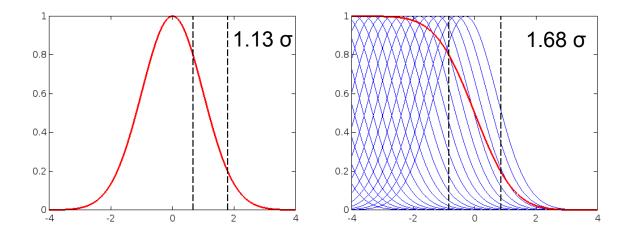


1. For a single spot:

 $LP \approx 1.13 \ \sigma$



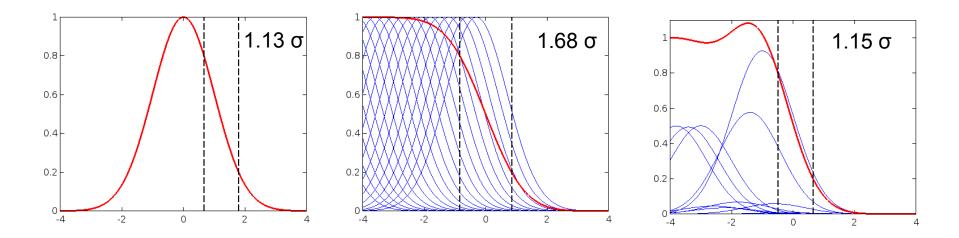




- 1. For a single spot: LP
- LP ≈ 1.13 σ
- 2. For equally weighted spots: LP \approx 1.68 σ



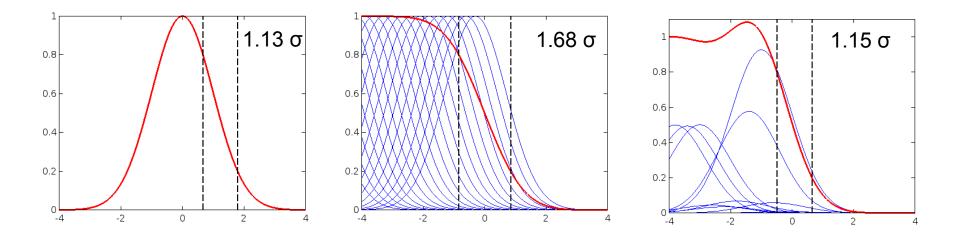




- 1. For a single spot: LP \approx 1.13 σ
- 2. For equally weighted spots: LP \approx 1.68 σ
- 3. Weights can be adjusted to recover sharpness, at the expense of uniformity: LP \approx 1.15 σ







1. For a single spot: $LP \approx 1$

LP ≈ 1.13 σ

- 2. For equally weighted spots: $LP \approx 1.68 \sigma$
- 3. Weights can be adjusted to recover sharpness, at the expense of uniformity: $LP \approx 1.15 \sigma$



Lateral dose profile characterization in scanning particle therapy

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Med. Phys. 38 (6), June 2011



Scanning spot size

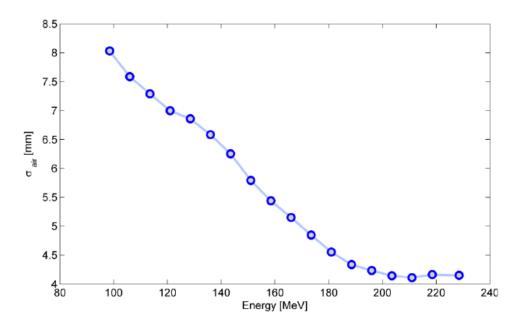
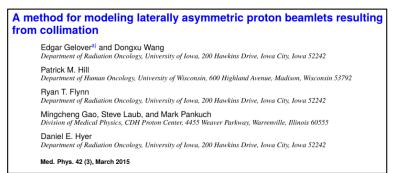


FIG. 2. Energy dependent spatial sigma for the IBA Universal Nozzle at CDH Proton Center. The same energy dependence was used for the Monte Carlo simulations.







Scanning spot size

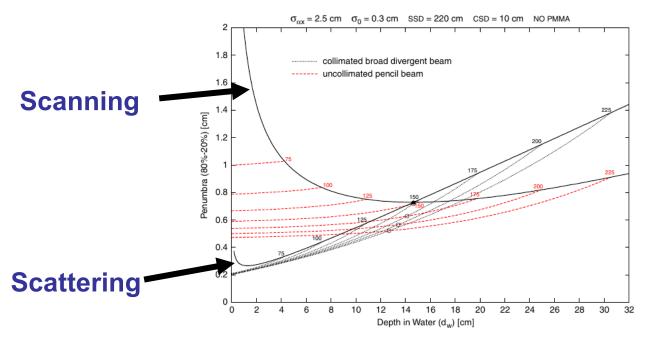


Figure 5. Penumbra as a function of depth in water (d_w) for different beam energies (expressed in MeV) for a collimated broad divergent beam and for an uncollimated pencil beam.

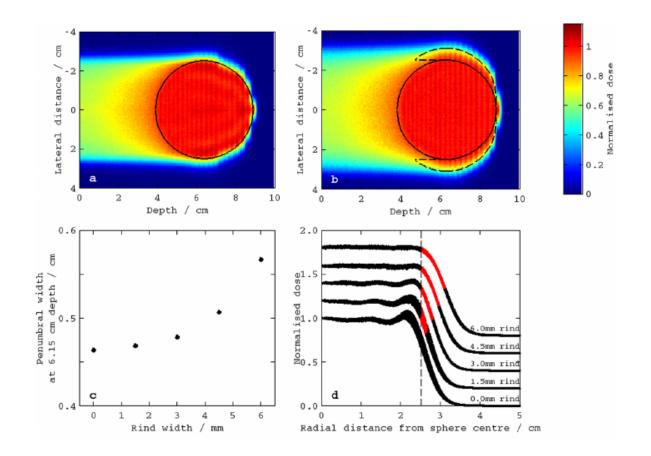
Phys. Med. Biol. 53 (2008) 1729–1750 doi:10.1088/0031-9155/53/6/016 Comparison between the lateral penumbra of a collimated double-scattered beam and uncollimated scanning beam in proton radiotherapy

Sairos Safai, Thomas Bortfeld and Martijn Engelsman

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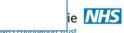


A Monte Carlo study on the collimation of pencil beam scanning proton therapy beams

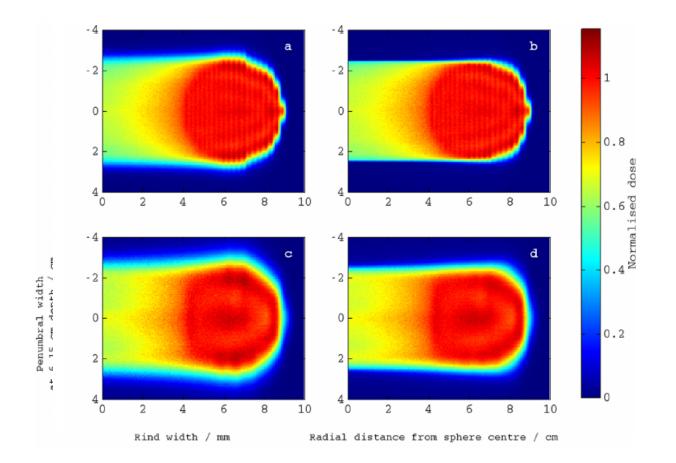
Frances C. Charlwood, Adam H. Aitkenhead,^{a)} and Ranald I. Mackay

Med. Phys. 43 (3), March 2016





Collimation of 3D volumes



A Monte Carlo study on the collimation of pencil beam scanning proton therapy beams

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Med. Phys. 43 (3), March 2016





Collimator implementation: Physical design

Phys. Med. Biol. 59 (2014) N187-N196

doi:10.1088/0031-9155/59/22/N187

Note

Effects of spot size and spot spacing on lateral penumbra reduction when using a dynamic collimation system for spot scanning proton therapy

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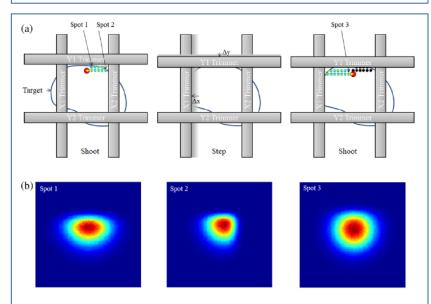


Figure 2. (*a*) A beam's eye view diagram illustrating the step-and-shoot delivery technique for positioning the trimmer blades to intercept the beam when it arrives at the edges of the target and (*b*) selected spot dose distributions qualitatively illustrating the effect of the trimmers on a single spot.

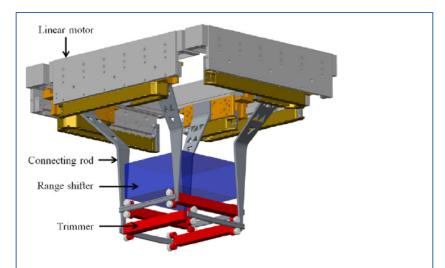


Figure 1. Major DCS components. The position of each trimmer is individually controlled by a linear motor that is connected to the trimmer via a connecting rod. A range shifter is also mounted just upstream of the trimmers. A support frame and housing surrounding the components is not shown.

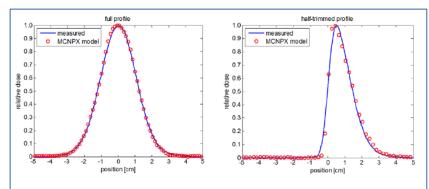
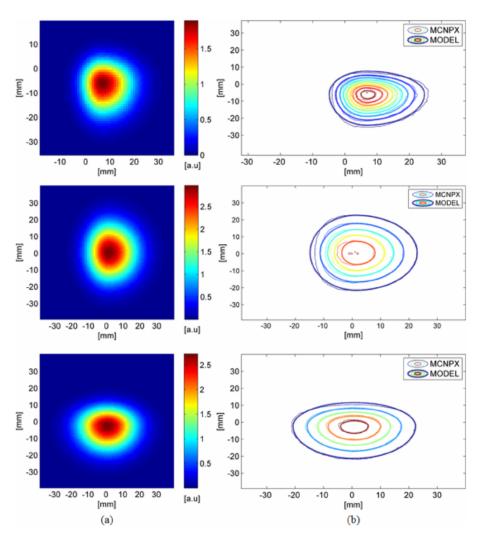


Figure 4. Experimental measurements of an untrimmed and half-trimmed profile to validate the Monte Carlo model.

Collimator implementation: Analytical dose models



A method for modeling laterally asymmetric proton beamlets resulting from collimation

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Med. Phys. 42 (3), March 2015



Fig. 6. (a) Examples of three modeled lateral dose distributions at the depth of the Bragg peak (5 cm) for the 128.0 MeV beam. (b) Isodose comparison with MCNPX in the beam's eye view. The trimmer configurations shown are identical to those in Fig. 5.

Clinical case studies

Is collimation needed?

- Case 1: Nasal cavity
- Case 2: Ewing sarcoma of cheek
- Case 3: Chordoma
- Case 4: Nasopharynx

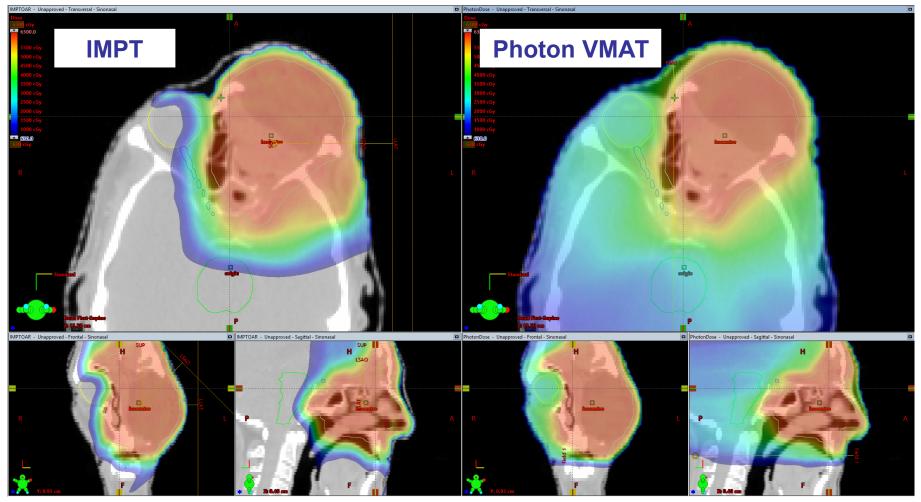
- Photon VMAT
- Passive scattered protons
- Photon IMRT
- Photon VMAT





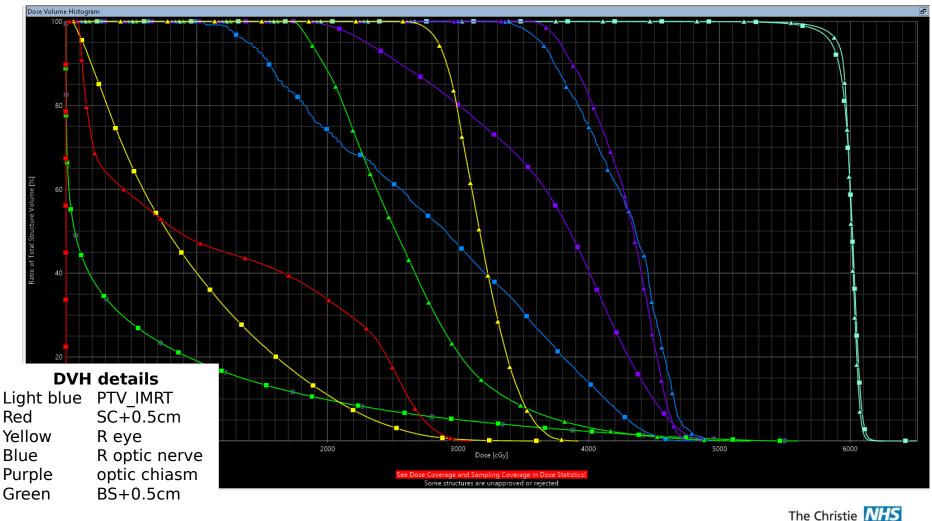
Clinical case 1: Nasal cavity

- Target is superficial and close to optics
- Locally advanced adenoid cystic carcinoma of the right sino-nasal anterior skull base region, treated by left partial maxillectomy
- Dose: 60 Gy



Clinical case 1: Nasal cavity

- IMPT sparing of contra-lateral optics is improved compared to photons.
- IMPT target coverage is comparable to photons.

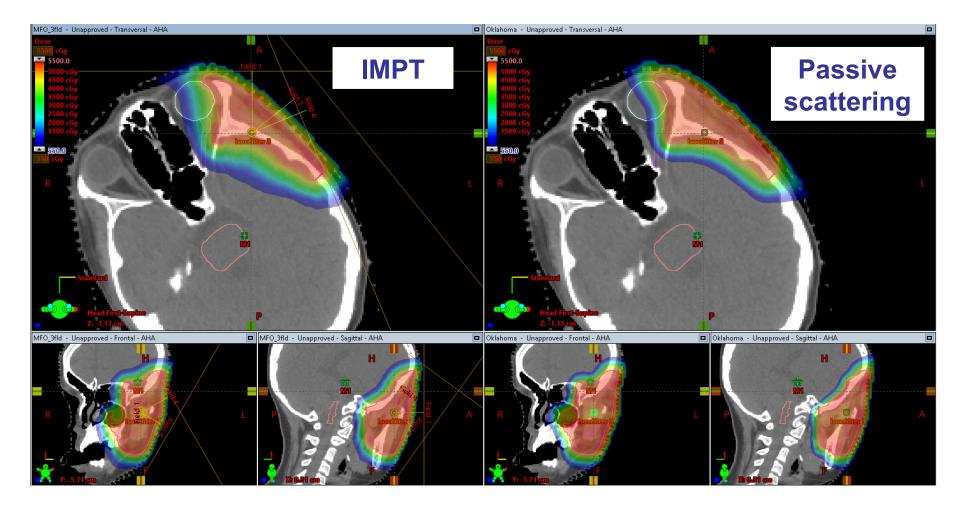


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Squares IMPT Triangles Photons

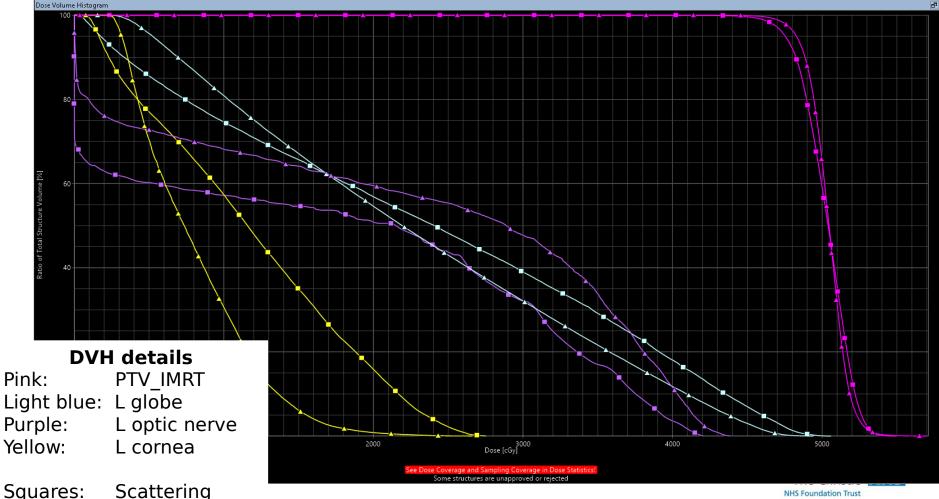
Clinical case 2: Ewing sarcoma

- Target is superficial and close to optics.
- 50.4 Gy



Clinical case 2: Ewing sarcoma

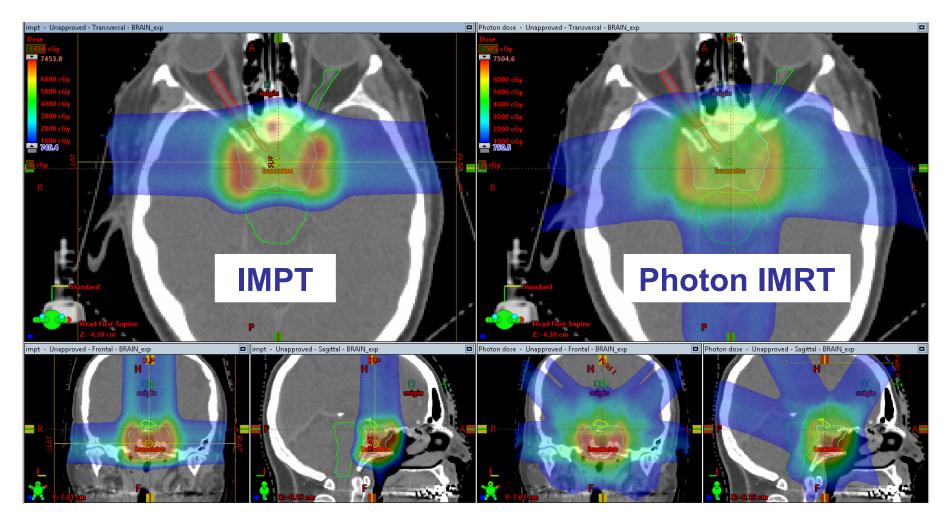
- IMPT target coverage is comparable to passive scattering.
- IMPT dose fall-off is less sharp around target.
- IMPT optic nerve dose is higher.



Triangles: IMPT

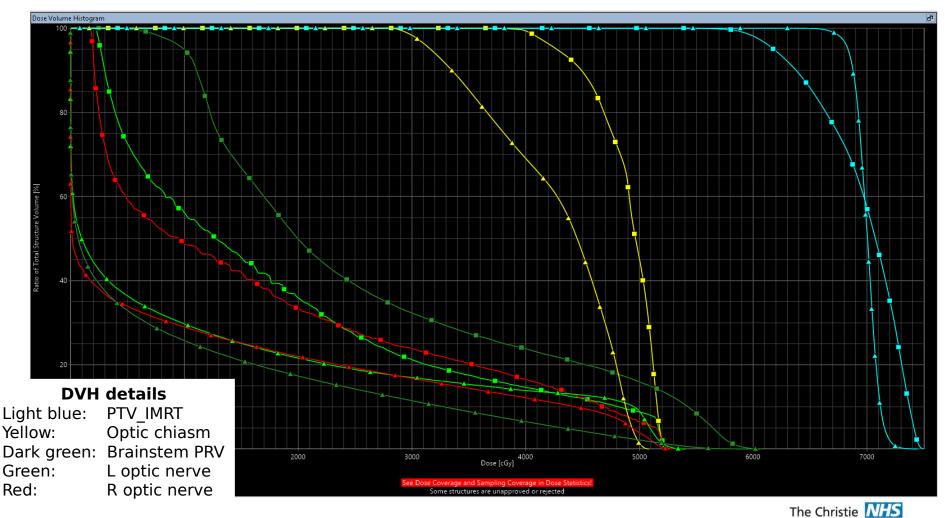
Clinical case 3: Chordoma

- Clinicians initially thought this case might be unsuitable for protons due to proximity of brainstem to target.
- 70 Gy.



Clinical case 3: Chordoma

- Control of dose to target is as good as (or better than) photons.
- IMPT sparing of OARs is improved compared to photons.



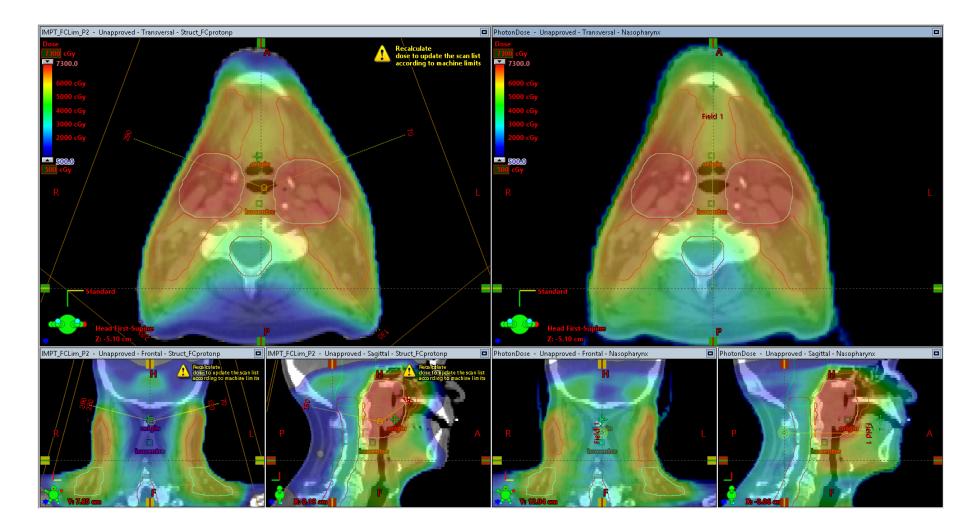
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Squares: Photons Triangles: IMPT



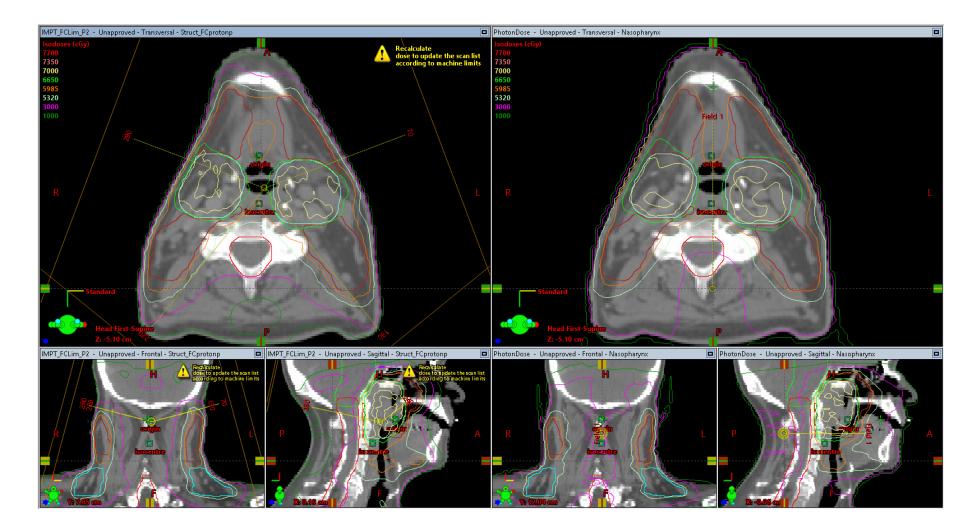








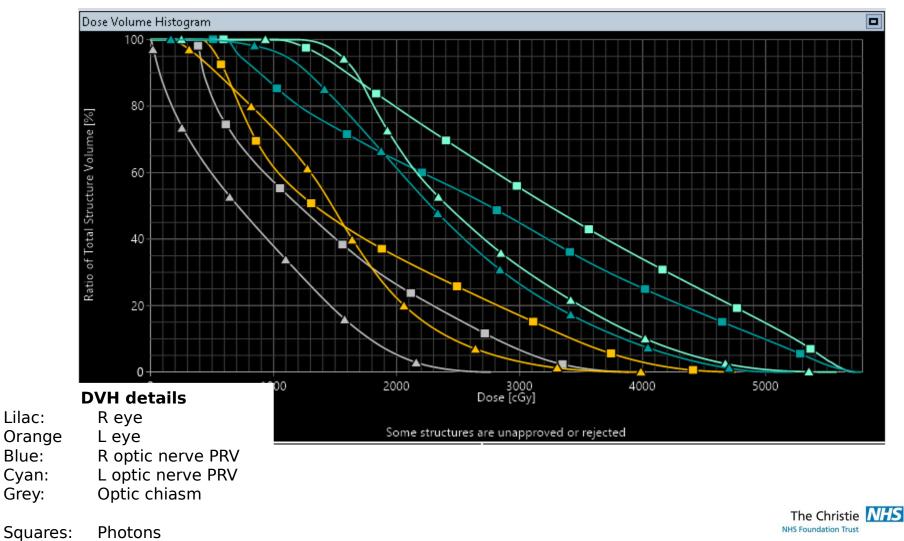








Optics: IMPT reduced dose



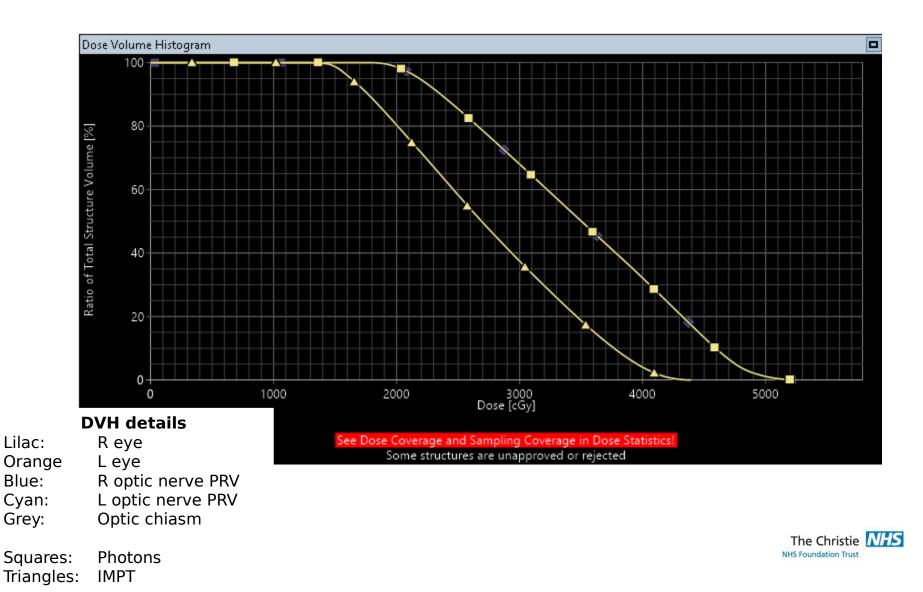
Triangles: IMPT

Lilac:

Blue:

Grey:

• Optic chiasm: IMPT reduced dose

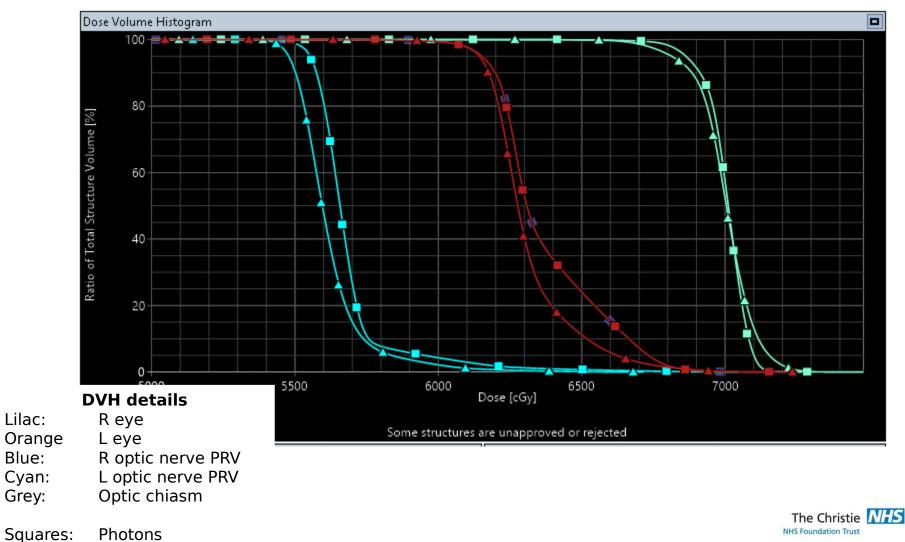


• Targets: 70, 63, 56 Gy

Triangles:

IMPT

• IMPT showed poorer uniformity



Summary

- Lateral penumbra is between 1.13 1.68 σ
- The optimizer can adjust spot weights to sharpen an edge at the cost of poorer uniformity (hot and cold spots).
- Current PBS technology is capable of producing similar plan quality as VMAT photons for the cases investigated here.

Potential for improvement:

- Collimation
- Reduced spot sizes
- Avoiding use of range shifter where possible





Thank you







