Monte Carlo simulations for research as well as clinical support in proton therapy





**R**ADIATION **O**NCOLOGY



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### Monte Carlo tools

Versatile

# Limited functionality

### Tasks







#### **Tool for Particle Simulation**



Perl J; Shin J; Schuemann S; Faddegon BA and Paganetti H: TOPAS - An innovative proton Monte Carlo platform for research and clinical applications. Medical Physics 2012 39: 6818-6837



University of California

San Francisco



NATIONAL ACCELERATOR LABORATORY

MGH

UC Davis eye treatment delivery system

MGH gantry treatment delivery system

Samsung Medical Center



Perl J; Shin J; Schuemann S; Faddegon BA and Paganetti H: TOPAS - An innovative proton Monte Carlo platform for research and clinical applications. Medical Physics 2012 39: 6818-6837







Shin J; Perl J; Schuemann S; Paganetti H and Faddegon BA: A modular method to handle multiple timedependent quantities in Monte Carlo simulations. Physics in Medicine and Biology 2012 57: 3295-3308







# Validation



Testa M; Schümann J; Lu H-M; Shin J; Faddegon B; Perl J and Paganetti H: Experimental validation of the TOPAS Monte Carlo system for proton therapy simulations. Medical Physics 2013 40: 121719





### Monte Carlo tools

Versatile

# Limited functionality









- Proton transport physics
  - Physics models

Kawrakow, *Med Phys*, **27**, 485(2000), Fippel *et. al., Med Phys*, **3**, 2263 (2004), Penelope manual (2009), Geant4 physics manual (2011)

- Multiple scattering and energy straggling
- Nuclear interaction is handled by an empirical strategy

Fippel et. al., Med Phys, 31, 2263(2004)

| (a)                   |              | 1.6                | TOPAS/Geant4<br>gPMC (b)                 |              | (c)   |
|-----------------------|--------------|--------------------|------------------------------------------|--------------|-------|
|                       | Source       | <i>&lt;σ/D&gt;</i> | $P_{\gamma}$                             | $P_{\gamma}$ | Т     |
|                       | Energy (MeV) | (%)                | (1mm/1%)(%)                              | (2mm/2%)(%)  | (sec) |
| Inhomogeneous phantom | 100          | 0.9                | 99.9                                     | 99.9         | 9.44  |
| Patient               | 100          | 1.0                | 95.1                                     | 99.9         | 10.08 |
|                       |              | -12                | -12 -4 4 12 -12 -4 4 12<br>x (cm) y (cm) |              |       |

Jia X; Schuemann J; Paganetti H and Jiang SB: GPU-based fast Monte Carlo dose calculation for proton therapy. Physics in Medicine and Biology 2012 57: 7783-7798











# Monte Carlo for Research

Example: New concepts using prompt gamma range verification





#### **Correlation of Prompt Gamma Rate Functions with position along an SOBP**



Testa; Min; Verburg; Schümann; Lu; Paganetti: Range verification in proton therapy based on the characteristic prompt-gamma timepatterns of passively modulated beams. Submitted



#### **Application to a Prostate Patient**



Testa; Min; Verburg; Schümann; Lu; Paganetti: Range verification in proton therapy based on the characteristic prompt-gamma timepatterns of passively modulated beams. Submitted



## Example:

New concepts using prompt gamma range verification

- Prompt Gamma Ray Functions can be determined by MC-simulations.
- 2mm range verification is achievable in a water phantom for a dose of 2.5cGy.
- For a typical prostate tumor treatment a 4mm resolution in range is achievable for a dose of 15cGy.
- Energy and TOF-selection simplifies the detection design and is effective in discriminating the promptgamma signal from the background.

Testa; Min; Verburg; Schümann; Lu; Paganetti: Range verification in proton therapy based on the characteristic prompt-gamma timepatterns of passively modulated beams. Submitted











# Monte Carlo for Clinical Research

Example 1: Understanding the interplay effect when treating lung cancer with pencil beam scanning











# Results for single fraction delivery attention: different scale







# Results for 35 fraction delivery attention: different scale







# Example 1: Understanding the interplay effect when treating lung cancer with pencil beam scanning

- Local control is preserved using a large spot size and conventional fractionation, but not for SBRT
- Small spots appear to be generally more sensitive to interplay effects
- Up to 10% loss in 12-month local control even for 30 fractions using small spots
- Tumors with high amplitudes relative to their size show more significant interplay
- There is significant patient variability depending on tumor location and size





# Monte Carlo for Clinical Research

# Example 2: The use of LET information in proton therapy treatment planning









DOSE



Sethi; Giantsoudi; Raiford; Rappalino; Caruso; Yock; Tarbell; Paganetti; MacDonald: Patterns of failure following proton therapy in medulloblastoma; LET distributions and RBE associations for relapses. International Journal of Radiation Oncology, Biology, Physics 2014 88: 655-663







Sethi; Giantsoudi; Raiford; Rappalino; Caruso; Yock; Tarbell; Paganetti; MacDonald: Patterns of failure following proton therapy in medulloblastoma; LET distributions and RBE associations for relapses. International Journal of Radiation Oncology, Biology, Physics 2014 88: 655-663





# Intensity-modulated proton therapy (IMPT)

# PLAN 1



Dose

5



# PLAN 2

Grassberger C; Trofimov A; Lomax A and Paganetti H: Variations in linear energy transfer within clinical proton therapy fields and the potential for biological treatment planning. International Journal of Radiation Oncology, Biology, Physics 2011 80: 1559-1566





# Biological dose optimization based on LET LET-guided multi-criteria optimization (MCO)



Giantsoudi; Grassberger; Craft; Niemierko; Trofimov; Paganetti: Linear energy transfer (LET)-Guided Optimization in intensity modulated proton therapy (IMPT): feasibility study and clinical potential. Int J Radiat Oncol Biol Phys 2013 87: 216-222





# **LET-guided MCO**



Giantsoudi; Grassberger; Craft; Niemierko; Trofimov; Paganetti: Linear energy transfer (LET)-Guided Optimization in intensity modulated proton therapy (IMPT): feasibility study and clinical potential. Int J Radiat Oncol Biol Phys 2013 87: 216-222





# Example 2: The use of LET information in proton therapy treatment planning

- For doses and LET values relevant in proton therapy, one can assume a close to linear relationship between LET and RBE for a given α/β. LET information can potentially be used to understand unexpected side effects
- LET information can be used as additional parameter in treatment optimization

Giantsoudi; Grassberger; Craft; Niemierko; Trofimov; Paganetti: Linear energy transfer (LET)-Guided Optimization in intensity modulated proton therapy (IMPT): feasibility study and clinical potential. Int J Radiat Oncol Biol Phys 2013 87: 216-222











# Uncertainties in predicting the beam range in patients

| Source of range uncertainty in the patient         | Range<br>uncertainty        |           |
|----------------------------------------------------|-----------------------------|-----------|
| Independent of dose calculation:                   |                             |           |
| Measurement uncertainty in water for commissioning | $\pm 0.3 \text{ mm}$        |           |
| Compensator design                                 | $\pm 0.2 \text{ mm}$        |           |
| Beam reproducibility                               | $\pm 0.2 \text{ mm}$        |           |
| Patient setup                                      | $\pm 0.7 \text{ mm}$        |           |
| Dose calculation:                                  |                             |           |
| Biology (always positive)                          | +0.8 %                      |           |
| CT imaging and calibration                         | $\pm 0.5$ %                 |           |
| CT conversion to tissue (excluding I-values)       | $\pm 0.5$ %                 |           |
| CT grid size                                       | $\pm 0.3$ %                 |           |
| Mean excitation energies (I-values) in tissue      | ± 1.5 %                     |           |
| Range degradation; complex inhomogeneities         | - 0.7 %                     |           |
| Range degradation; local lateral inhomogeneities * | ± 2.5 %                     |           |
| Total (excluding *)                                | 2.7% + 1.2 mm               | Typical   |
| Total                                              | <b>4.6%</b> + <b>1.2</b> mm | Worst cas |

H. Paganetti: Range uncertainties in proton beam therapy and the impact of Monte Carlo simulations. Phys. Med. Biol. 57: R99-R117 (2012)



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| Range degradation; local lateral inhomogeneities * | ± 2.5 %                     | → ± 0.1 %          |  |
| <b>Total (excluding *)</b> 2.7% +                  |                             | $24\% \pm 12$ mm   |  |
| Total                                              | <b>4.6%</b> + <b>1.2</b> mm | 2.7 /0 T 1.2 IIIII |  |

H. Paganetti: Range uncertainties in proton beam therapy and the impact of Monte Carlo simulations. Phys. Med. Biol. 57: R99-R117 (2012)



## Uncertainties in predicting the beam range in patients



Prescribed range in cm

H. Paganetti: Range uncertainties in proton beam therapy and the impact of Monte Carlo simulations. Phys. Med. Biol. 57: R99-R117 (2012)



Range differences between analytical and Monte Carlo based dose calculation analyzed by comparing distal dose surfaces in patients

# **Dose Distributions** a TOPAS d XiO

**TOPAS-XiO** 



Field with an average range difference of <0.1mm but a root-meansquare deviation of 4.7mm

0.1 [Gy(RBE)]



Schuemann, Dowdell, Min, Paganetti: Site-specific range uncertainties caused by dose calculation algorithms for proton therapy: Phys. Med. Biol. submitted



# Estimation of range uncertainties by performing MC dose calculation on 508 fields



includes uncertainties from sources other than dose calculation

Schuemann, Dowdell, Min, Paganetti: Site-specific range uncertainties caused by dose calculation algorithms for proton therapy: Phys. Med. Biol. submitted





# Monte Carlo for Clinical Use

- Monte Carlo in routine dose calculation has the potential to reduce treatment margins
- Monte Carlo can be used to revise current margins and better understand uncertainties due to dose calculation







MGH Radiation Oncology Physics Research team

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- Federal Share on C06 CA059267
  "Accurate Monte Carlo Dose Calculation for Proton Therapy Patients"
- MGH ECOR
  "Biologically Optimized Treatment Planning for Proton Beam Therapy"



